

# A Blood Gene Expression Marker of Early Alzheimer's Disease

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**Abstract.** A marker of Alzheimer's disease (AD) that can accurately diagnose disease at the earliest stage would significantly support efforts to develop treatments for early intervention. We have sought to determine the sensitivity and specificity of peripheral blood gene expression as a diagnostic marker of AD using data generated on HT-12v3 BeadChips. We first developed an AD diagnostic classifier in a training cohort of 78 AD and 78 control blood samples and then tested its performance in a validation group of 26 AD and 26 control and 118 mild cognitive impairment (MCI) subjects who were likely to have an AD-endpoint. A 48 gene classifier achieved an accuracy of 75% in the AD and control validation group. Comparisons were made with a classifier developed using structural MRI measures, where both measures were available in the same individuals. In AD and control subjects, the gene expression classifier achieved an accuracy of 70% compared to 85% using MRI. Bootstrapping validation produced expression and MRI classifiers with mean accuracies of 76 and 82%, respectively, demonstrating better concordance between these two classifiers than achieved in a single validation population. We conclude there is potential for blood expression to be a marker for AD. The classifier also predicts a large number of people with MCI, who are likely to develop AD, are more AD-like than normal with 76% of subjects classified as AD rather than control. Many of these people do not have

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overt brain atrophy, which is known to emerge around the time of AD diagnosis, suggesting the expression classifier may detect AD earlier in the prodromal phase. However, we accept these results could also represent a marker of diseases sharing common etiology.

Keywords: Alzheimer's disease, biomarkers, blood, diagnosis, gene expression pattern analysis, leukocytes, magnetic resonance imaging, mild cognitive impairment

Supplementary data available online: <http://www.j-alz.com/issues/33/vol33-3.html#supplementarydata03>

## INTRODUCTION

Alzheimer's disease (AD) is a common chronic neurodegenerative disorder, accounting for ~60% of dementia cases. Dementia affects 63 million patients worldwide with numbers set to rise to 114 million by 2050 resulting in dramatic social and economic consequences as our care systems struggle to cope [1]. Although much progress has been made in understanding the molecular pathology of AD, the treatments currently available only temporarily alleviate some symptoms and do not modify pathology. The use of biomarkers for identification of individuals with AD prior to the appearance of clinical symptoms, the so-called pre-dementia phase of the disease [2], will be essential to the development of drugs for early intervention [3–5]. Furthermore, if sufficiently powered, some biomarkers could be used as part of a screening program for at-risk elderly people [6].

By the time an individual is diagnosed with AD, there is already considerable neuronal cell loss, plaque deposition, and neurofibrillary tangles within the brain [7, 8], which may have emerged up to 10 years or more before clinical diagnosis [9–11]. Biomarkers linked to the pathophysiological process in AD can greatly increase the confidence of concluding a person will have an AD-endpoint even in the pre-dementia phase [12]. Cerebrospinal fluid (CSF) biomarkers such as increased tau and decreased levels of amyloid- $\beta$  ( $A\beta$ )<sub>1-42</sub> in the CSF correlate with postmortem AD pathology [13, 14]. These measurements together not only differentiate AD from normal elderly controls with high accuracy, but can also predict which subjects with mild cognitive impairment (MCI) are likely to progress to AD within 5 years [15]. However, a lumbar puncture to collect CSF is an invasive procedure, which may not be suitable for use in large-scale trials or for screening populations. Similarly, positron emission tomography (PET) imaging of amyloid burden in the brain correlates with clinical diagnosis of AD,  $A\beta$  neuropathology at autopsy [13, 14, 16], and CSF  $A\beta$ <sub>1-42</sub> levels [17–20]. PET imaging is expensive and

impractical to be used in large groups of frail elderly patients and may be restricted to specialist centers.

Although AD is a disease of the brain, it is increasingly accepted that there is communication between the brain and the periphery, and we therefore hypothesize that there will be blood-associated changes detectable in disease which could be used to develop a diagnostic marker. Blood is easily obtainable in frail elderly people and relatively inexpensive to analyze, making it an attractive source for developing a biomarker [21]. Many studies, including those from our own group, have identified AD- and/or MCI-related protein changes in blood plasma using 2DGE/Mass Spectrometry and luminex technology [22–30], and are undergoing further rounds of testing to establish their validity as the basis for an accurate marker. Furthermore, companies specializing in AD diagnostics have recently published reports of gene expression changes in blood that are able to distinguish AD subjects from cognitively normal people. Diagenic ASA published a discovery and validation study consisting of a 96 gene classifier with 72% accuracy for AD diagnosis. The marker could also correctly predict the outcome of 7 out of 10 MCI subjects after a 2 year follow-up. Although these numbers are too small to draw firm conclusions about its performance in identifying pre-dementia in MCI subjects, these results are encouraging [31, 32]. ExonHit Therapeutics used the additional splice variant discriminatory power of Genome-Wide Splice Arrays to identify a blood expression classifier consisting of 133 genes able to distinguish AD from normal elderly control subjects with 98% accuracy [33]. Combining blood measures across different modalities such as proteins, metabolites, and gene expression may further improve biomarker accuracy, although the outcomes of these studies have yet to be reported.

Our aim was to first identify and validate an AD diagnostic gene expression marker in blood able to distinguish people clinically diagnosed with AD from normal elderly controls with high sensitivity and specificity. We then sought to evaluate its specificity

115 and sensitivity compared to another marker which  
116 incorporates structural magnetic resonance imaging  
117 (MRI) measures of regional brain atrophy and cortical  
118 thickness assessed in the same individuals, using  
119 a hypothesis-free approach. To date, the outcome of  
120 comparing a gene expression marker of AD alongside  
121 a classifier using measures of brain atrophy has not yet  
122 been reported. Classifiers combining measures of cortical  
123 thickness and/or regional brain atrophy changes  
124 in AD have previously been shown to very accurately  
125 distinguish AD from normal elderly controls [34].  
126 Structural brain changes can also be used to identify  
127 people with MCI who will subsequently receive  
128 a diagnosis of AD or experience a more rapid drop  
129 in Mini-Mental Status Examination (MMSE) score  
130 over time [35, 36]. Structural brain changes generally  
131 appear after changes in other modalities such as CSF  
132 A $\beta$  and tau and coincide with neuronal cell loss and  
133 the onset of clinical symptoms [11, 37].

134 Individuals with MCI are likely to have an AD-  
135 endpoint and therefore are more likely to be classified  
136 as AD-like rather than normal using an appropriate  
137 biomarker. The proportion of people with MCI having  
138 prodromal AD varies between studies as it depends on  
139 the method of ascertainment, the criteria for identifying  
140 people with MCI, the period of follow-up, and the  
141 confirmatory methods for subsequent AD diagnosis.  
142 Typical estimates suggest around ~40–75% of people  
143 who have cognitive symptoms consistent with MCI  
144 will eventually progress to pathologically confirmed  
145 AD [38–40], with only ~5% “reverting” to normal  
146 [41, 42] and ~30–55% developing other dementias  
147 [43–45]. We were therefore interested to investigate  
148 whether a set of blood gene expression changes found  
149 in AD patients also exist in a MCI population and  
150 whether or not there was any distinction between MCI  
151 subjects close to receiving a clinical diagnosis of AD  
152 and those who remained MCI within the subsequent  
153 two year follow-up period. While our AD diagnostic  
154 classifier was adequately powered, we did not have sufficient  
155 power to build a separate predictive classifier within  
156 our MCI population to predict which subjects  
157 would develop AD within a two-year period.

## 158 METHODS AND MATERIALS

### 159 *Clinical subjects and samples*

160 Subjects used were from AddNeuroMed, a  
161 large cross-European prospective biomarker study  
162 (2005–2007) [46, 47]. Informed consent was obtained  
163 for all subjects according to the Declaration of Helsinki

164 (1991) and protocols and procedures were approved  
165 by the relevant local ethical committees at each site.  
166 Subjects were excluded from the study if they were  
167 younger than 65 years, had significant neurological or  
168 psychiatric illness other than AD, significant unstable  
169 systematic illness or organ failure, or a geriatric  
170 depression rating scale score  $\geq 4/5$  [48].

171 Normal elderly control subjects were recruited from  
172 non-related family members of AD patients, care-  
173 givers' relatives, social centers for the elderly, or GP  
174 surgeries and had no evidence of cognitive impairment.  
175 A small number of individuals recruited in this  
176 way met the MCI criteria detailed below and were  
177 therefore included in the MCI cohort for analyses.  
178 AD and MCI subjects were recruited primarily from  
179 local memory clinics, and as such the MCI cohort was  
180 expected to be composed largely of subjects with a  
181 likely AD-endpoint. AD subjects were diagnosed using  
182 the National Institute of Neurological and Commu-  
183 nicative Disease and Stroke and Alzheimer's disease  
184 (NINCDS-ADRDA) [49] and Diagnostic and Statistical  
185 Manual of Mental Disorders (DSM-IV) [50] criteria  
186 for possible or probable AD. All MCI subjects reported  
187 problems with memory, corroborated by an informant,  
188 but had normal activities of daily living as specified  
189 in the Petersen's criteria for amnesic MCI [51, 52].  
190 MCI subjects scored 0.5 on the total Clinical Dementia  
191 Rating Scale or had a memory score of 0.5 or 1 [53].  
192 Within 2 years of the baseline visit, some MCI subjects  
193 progressed to a clinical diagnosis of AD (MCI<sub>c</sub>), while  
194 others remained MCI (MCI<sub>nc</sub>). Diagnoses were made  
195 by trained researchers following a previously validated  
196 protocol [54].

197 All subjects underwent a structured interview and  
198 a battery of neuropsychological assessments including  
199 the Mini Mental State Examination (MMSE) [55],  
200 Global Deterioration Scale (GDS) [56], and Clinical  
201 Dementia Rating Scale (CDR) [53] by trained  
202 researchers. Control and MCI subjects were further  
203 assessed using the CERAD battery [57]. Detailed  
204 information on subject recruitment and assessments  
205 can be found in other published studies [46, 47].  
206 Where possible, whole blood samples were collected  
207 from each subject for DNA (*APOE* genotyping) and  
208 RNA analyses (gene expression). Consecutive subjects  
209 who met MRI inclusion criteria (no claustrophobia, no  
210 trauma or surgery which may have left ferromagnetic  
211 material in the body, ferromagnetic implants or pace-  
212 makers, and the ability to lie still for at least one hour)  
213 were invited to undertake an MRI scan until a total  
214 of ~20 subjects per diagnostic group per center were  
215 scanned.

216 *Whole blood RNA extraction*

217 Venous blood (2.5 ml) was collected into a  
 218 PAXgene™ Blood RNA tube (BD) for RNA analysis  
 219 from subjects who had fasted 2 hours prior to col-  
 220 lection. The sample was frozen at  $-20^{\circ}\text{C}$  overnight  
 221 and then transferred to  $-80^{\circ}\text{C}$  for long-term storage.  
 222 Prior to RNA extraction, samples were thawed at room  
 223 temperature overnight. RNA was extracted using the  
 224 PAXgene™ Blood RNA Kit (Qiagen), according to  
 225 the manufacturer's protocol. The yield and quality of  
 226 extracted RNA were assessed using the NanoDrop™  
 227 1000 spectrophotometer (NanoDrop Technologies)  
 228 and the Agilent 2100 Bioanalyzer (Agilent Technolo-  
 229 gies) respectively. Only samples with an RNA Integrity  
 230 Number  $\geq 7.0$  were analyzed in this study.

231 *Microarray analysis*

232 Illumina Human HT-12 v3 Expression BeadChips  
 233 (Illumina) were used to analyze whole genome tran-  
 234 script expression according to the protocol supplied  
 235 by the manufacturer for 356 subjects (116 control, 127  
 236 MCI, and 113 AD). Samples from subjects who had  
 237 also undergone an MRI scan or who had subsequently  
 238 changed their diagnosis from MCI to AD within 2  
 239 years of the sample being analyzed were prioritized for  
 240 inclusion. The remaining control, MCI, and AD sub-  
 241 jects were randomly chosen from the cohort available  
 242 at the time of analysis to provide roughly equal num-  
 243 bers across the three groups and to allow 356 samples  
 244 to be analyzed in total, a number chosen for practi-  
 245 cal reasons. The beadchips contained 48,803 probes  
 246 designed using data from RefSeq (Build 36.2, Rel  
 247 22) and the UniGene (Build 199) databases. Briefly,  
 248 the TotalPrep RNA Amplification Kit (Ambion) was  
 249 used to synthesize cDNA from 200 ng total RNA fol-  
 250 lowed by amplification and biotinylation of cRNA and  
 251 hybridization. Following hybridization, gene expres-  
 252 sion values were variance-stabilization transformed  
 253 and quantile normalized using the R Bioconductor  
 254 package lumi [58]. A total of 30 chips were excluded  
 255 from further analysis for a number of reasons includ-  
 256 ing very low BeadChip detection rate, disparity in  
 257 *XIST* gene expression gender calling (Illumina probe  
 258 ID: ILMN\_1764573) with recorded gender and/or gen-  
 259 der markers derived from SNP chip data from the  
 260 same individuals or diagnostic re-classification at sub-  
 261 sequent visits prior to final data analysis (other than  
 262 MCI-AD). This left a total of 326 subjects (104  
 263 AD, 118 MCI [77 MCI<sub>nc</sub>, 41 MCI<sub>c</sub>], and 104 nor-  
 264 mal elderly control subjects) which were used for

265 classifier development and validation. Probes that were  
 266 not expressed in any samples were removed from fur-  
 267 ther analysis, leaving 38,311 probes for classification  
 268 purposes. Data were adjusted for the independent vari-  
 269 ables of age, gender, collection site, and RNA quality  
 270 (RIN).

271 *Neuroimaging*

272 Highly automated bilateral regional cortical thick-  
 273 ness measures from 34 areas and regional brain volume  
 274 measures from 41 areas totaling 109 measures were  
 275 obtained from subjects who underwent MRI. Detailed  
 276 information about data acquisition, pre-processing,  
 277 and quality control assessment have been described  
 278 for this cohort in detail elsewhere [34, 36, 47, 59, 60].  
 279 Data from 91 AD, 92 MCI, and 90 control subjects  
 280 were included in the analyses.

281 *Diagnostic classifier development*

282 Using the clinical diagnosis of AD as the diagnos-  
 283 tic standard, we developed a classifier containing those  
 284 measures of blood gene expression able to achieve the  
 285 greatest sensitivity and specificity in a training cohort.  
 286 We based our methods on those recommended by the  
 287 MicroArray Quality Control II (MAQC-II) study [61].  
 288 Samples from AD and normal elderly control subjects  
 289 were randomly divided in to a 75% training cohort  
 290 (78 AD, 78 Control; Table 1) and a 25% independent  
 291 validation cohort (26 AD, 26 Control; Table 1). Ini-  
 292 tially a *t*-test was performed in the training cohort to  
 293 reduce the number of gene expression features, leav-  
 294 ing a total of 203 probes with *p*-value  $< 0.01$  (False  
 295 discovery rate (FDR)-corrected). These 203 probes  
 296 were then used to optimize the parameters of a random  
 297 forest model as the Random Jungle [62] implementa-  
 298 tion requires. In the optimization procedure, various  
 299 combinations of the random forest parameters includ-  
 300 ing mTry (number of randomly selected variables) and  
 301 nTrees (number of trees) were used. In addition,  
 302 we applied the Meng score as a measure of  
 303 variable importance [63], backward elimination, and  
 304 a conditional importance setting of 0.8, which was  
 305 kept constant throughout the optimization procedure.  
 306 The best training result was achieved by a setting of  
 307 nTrees = 750 and mTry = 15, with 50 probes included  
 308 in the model. These settings and the 50 highest ranked  
 309 probes were taken further into the final model. The  
 310 final optimized random forest parameters, 50 highest  
 311 ranked probes, and all samples in the training cohort  
 312 were then used to build a final random forest model,

Table 1  
Subject characteristics of the out of bag (training) and validation (test) cohorts used in the development of an AD-Control classifier

AD-Control classifier subject characteristics	Out of bag cohort (Training)		Validation cohort (Test)			
	Control	AD	Control	MCI <sub>inc</sub>	MCI <sub>c</sub>	AD
Samples used in analysis	78	78	26	77	41	26
Gender (F/M)	45/33	52/26	17/9	38/39	27/14	20/6
No. with MRI measures	67	68	23	73	19	23
Age in years ( $\pm$ SD)	72.1 (6.2)	75.5 (6.9)	73.2 (7.0)	74.3 (5.7)	75.0 (6.2)	75.1 (6.4)
Disease duration in years ( $\pm$ SD)	N/A	3.7 (2.5)	N/A	N/A	N/A	4.0 (2.3)
MMSE ( $\pm$ SD)	29.0 (1.2)	21.1 (4.4)	29.2 (1.3)	27.3 (1.7)	26.2 (2.2)	20.5 (5.1)
ADAS-Cog ( $\pm$ SD)	N/A	23.6 (9.4)	N/A	N/A	N/A	22.9 (11.2)
CDR sum of boxes ( $\pm$ SD)	0.1 (0.2)	6.4 (3.0)	0.1 (0.2)	1.3 (0.8)	2.1 (1.1)	7.0 (3.7)

which was then tested with the independent validation cohort.

In order to allow us to directly compare the predictive power of gene expression with sMRI, we re-developed the expression classifier to include only those samples for which both imaging and gene expression data were available. AD and normal elderly control subjects were divided into a 75% training cohort (68 AD, 67 Control; Table 1) and a 25% independent validation cohort (23 AD, 26 Control; Table 1), maintaining sample groups as before and removing those where only expression data were available in order to achieve a similar sample distribution across training and test cohorts. The reduced training cohort was then used to develop three additional diagnostic models; the first included only sMRI imaging measures, the second included sMRI and gene expression, and the third only gene expression in these samples. For all three models, MCI samples were included with the validation cohort. For imaging classifier development, the 109 structural brain measures derived from MRI were used to optimize the parameters of a random forest model as before with the 20 highest ranked measures taken further in to the final model. For the combined sMRI and gene expression model, 30 imaging and 45 gene expression measures were in the model and for the gene expression model using samples with available sMRI measures, there were 50 measures. The sample workflow, analysis, and model development scheme for classification is illustrated in Fig. 1.

All four diagnostic models were further validated by bootstrapping. First the data set was randomly split into a bootstrap training-set (75% of samples) and a bootstrap test-set (25% of samples). Each bootstrap training-set was used to build a random forest model, which was subsequently tested in the bootstrap test-set. Thus overall, 200 bootstrap random forest models were generated and tested. The bootstrapping

procedure generated a list summarizing and ranking probes based on their importance and predictive power across the 200 bootstrap models.

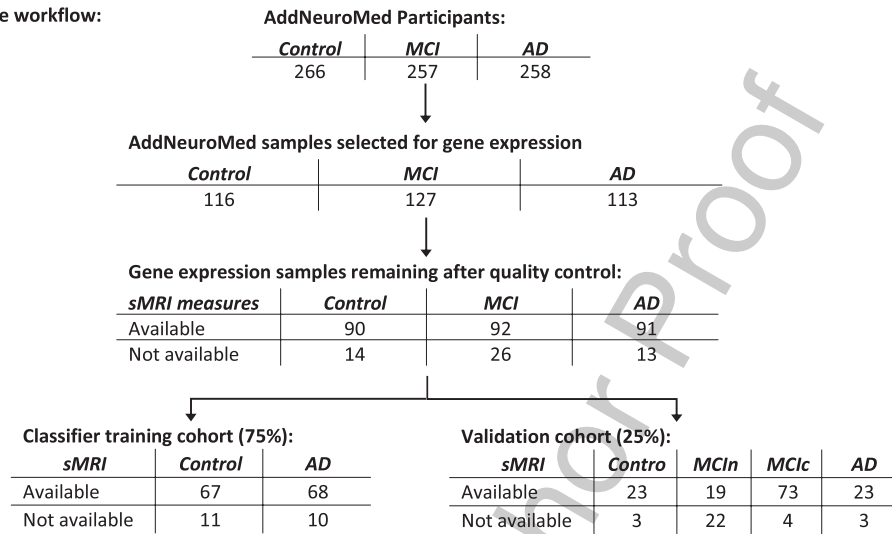
Using the R package MVpower (<http://cran.r-project.org/web/packages/MVpower/MVpower.pdf>) in the above approach, we estimate that for effect sizes of 0.7 and 0.2 we have power of 100 and 80% respectively to develop a Random Forest classifier with 203 features and 50 probes based on sample sizes of 78 in each group. Our effect size of 0.7 was based on differences between cases and controls in the selected 203 features, 0.2 was chosen as a conservative lower limit.

## RESULTS

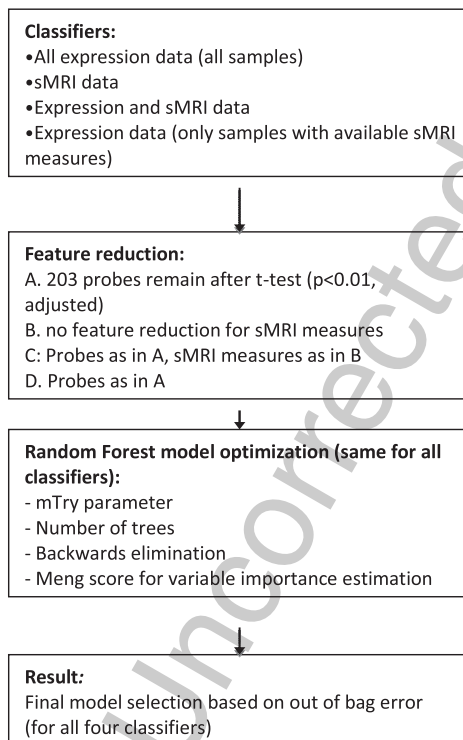
### *Performance of diagnostic classifier in distinguishing AD from normal elderly control subjects*

We sought to identify and evaluate a blood gene expression diagnostic classifier of AD that could distinguish people with AD from normal elderly control subjects. We found 48 genes, represented by 50 Illumina probes selected through backward elimination of 203 probes identified by *t*-tests (Supplementary Table 2; available online: <http://www.j-alz.com/issues/33/vol33-3.html#supplementarydata03>), and achieved the highest "out of bag" accuracy in our training cohort. The 50 probes along with their Meng score of relative importance within the classifier are listed in Table 2. When this AD-Control classifier was applied to the independent validation group of samples, it was able to correctly classify 39/52 subjects (75.0% accuracy), of which 21/26 AD subjects were correctly classified (80.8% sensitivity) and 18/26 normal elderly control subjects were correctly excluded (69.2% specificity) (Table 3A), achieving a positive predictive value (PPV) of 72.4% and negative

## 1. Sample workflow:



## 2. Use of training cohort for classifier development:



## 3. Final validation of classifiers:

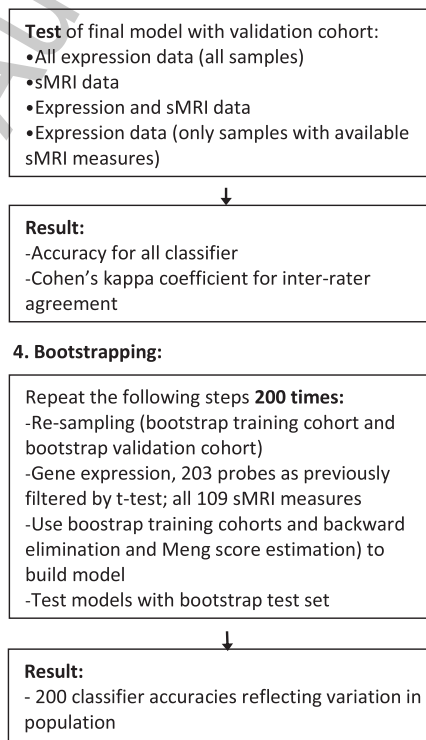


Fig. 1. Sample flow, model development, and model validation scheme for classification. Samples with a minimum RNA integrity number of 7 were selected from AddNeuroMed participants, with priority given to those who had undergone MRI scans and MCI subjects known to have converted from MCI to AD. The remaining control, MCI, and AD subjects were randomly chosen from available samples to provide approximately equal numbers across the three groups. When generating the AD-Control classifier, AD and Control samples were randomly categorized as training (out of bag) (75%) or validation (25%) from samples passing quality control. Samples from all MCI subjects were examined as part of the validation cohort to assess how they were categorized relative to AD and normal elderly control subjects. Each classifier was developed in the training cohort and then tested in the validation cohorts to generate a final probe (gene) or imaging measure list along with a measure of accuracy, sensitivity, and specificity. Finally data underwent bootstrapping, whereby in each bootstrap iteration (total of 200) a new development and validation set was drawn from the complete data set used for each model. In each round of bootstrapping, the training set was used to build a classification model, which was then assessed with the validation set. This method gives a range of classifier accuracies, reflecting variation in the population, and allowing an additional assessment to the traditional independent test set approach.

Table 2  
The 50 Illumina probes (48 genes) that best classify AD from control samples in the training cohort

Gene symbol	Illumina probe	Meng score <sup>a</sup>	<i>q</i> -value <sup>b</sup>	Bootstrap count <sup>c</sup>
RPS27A	ILMN_2048326	1.87E-02	2.11E-05	200
CHMP4A	ILMN_1715607	1.71E-02	4.10E-03	200
SFRS17A	ILMN_1807737	1.68E-02	1.97E-03	198
POMP	ILMN_1693287	1.67E-02	3.62E-05	147
C5ORF41	ILMN_2195821	1.66E-02	9.41E-05	142
FTHL7	ILMN_2234016	1.65E-02	2.28E-03	67
LOC401206	ILMN_1792528	1.59E-02	3.62E-05	115
AK2	ILMN_1716053	1.58E-02	2.34E-03	161
UQCRB	ILMN_1759453	1.55E-02	3.64E-03	200
LOC653505	ILMN_1776260	1.55E-02	4.95E-05	134
PGS1	ILMN_2075051	1.51E-02	2.34E-03	58
NRBP2	ILMN_1733248	1.50E-02	1.85E-03	197
UTP14A	ILMN_2095820	1.47E-02	2.34E-03	57
DICER1	ILMN_1772692	1.46E-02	4.32E-04	180
RPL36AL	ILMN_2189936	1.44E-02	3.62E-05	200
ATP5EP2	ILMN_2225887	1.42E-02	5.76E-03	145
SIRPG	ILMN_1771801	1.39E-02	2.34E-03	20
LSM3	ILMN_2229242	1.36E-02	8.15E-03	200
APBB3	ILMN_2320513	1.33E-02	2.89E-03	177
MRPL51	ILMN_2097421	1.32E-02	2.19E-07	200
RELL2	ILMN_1652540	1.30E-02	5.10E-03	187
CETN2	ILMN_1695645	1.29E-02	2.11E-05	195
PWP1	ILMN_1743049	1.18E-02	5.07E-03	81
KIAA0146	ILMN_1887174	1.15E-02	7.55E-04	100
LOC388720	ILMN_1754990	1.14E-02	2.12E-04	101
CIP29	ILMN_1680967	1.11E-02	5.41E-03	191
LOC388621	ILMN_1677262	1.11E-02	4.75E-03	139
SFRS17A	ILMN_2117716	1.10E-02	4.87E-04	182
PCBP1	ILMN_1673215	1.09E-02	4.23E-04	100
ATP5J2	ILMN_2310621	1.08E-02	3.09E-05	65
H2AFY	ILMN_2373495	1.07E-02	6.30E-03	163
COX17	ILMN_2187718	1.07E-02	1.21E-05	5
IDS	ILMN_1758626	1.07E-02	2.34E-03	162
SHFM1	ILMN_2128128	1.07E-02	2.80E-04	173
LOC651064	ILMN_1782417	1.03E-02	6.09E-03	53
STX16	ILMN_1741942	9.95E-03	1.91E-03	160
GDPD1	ILMN_2106265	9.93E-03	4.88E-03	179
C6ORF166	ILMN_2148847	9.85E-03	5.31E-03	27
ING3	ILMN_2237746	9.83E-03	5.42E-03	158
CACNA2D4	ILMN_1696317	9.61E-03	7.73E-03	47
PLEK	ILMN_1795762	9.22E-03	2.84E-03	3
NDUFA1	ILMN_1784286	9.04E-03	2.45E-06	198
CDKN1B	ILMN_1722811	7.90E-03	7.93E-03	199
RGS19	ILMN_1677085	7.62E-03	5.48E-03	165
RPS27A	ILMN_1755883	7.61E-03	2.77E-04	180
LOC731640	ILMN_1661174	7.41E-03	8.33E-03	66
AHSA1	ILMN_1703617	6.98E-03	1.74E-03	58
BXDC1	ILMN_1664167	6.43E-03	4.29E-04	0
KARS	ILMN_1777584	5.54E-03	2.56E-03	5
UBE2G1	ILMN_1814465	-4.62E-04	1.74E-03	105

<sup>a</sup>An estimate of variable (probe) importance in the AD versus Control classifier Random Forest model. <sup>b</sup>*q*-value from a *t*-test comparing AD and control samples. <sup>c</sup>The number of times each probe appeared in the 200 bootstrap iterations.

388 predictive value (NPV) of 78.3%. As *APOEε4* dosage  
389 is a known risk factor for developing AD, we repeated  
390 the model creation step including the *APOEε4*  
391 genotype in the list of attributes. During backward  
392 elimination, we found this attribute was removed in

the early rounds of the iterative process and therefore  
excluded it from further analysis. As the accuracy of a  
classifier varies depending on the population sampled,  
we bootstrapped the sampled population 200 times  
to assess the accuracy of the 203 probes identified

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Table 3  
Classifiers' performance in out of bag and validation data sets following Random Forests modeling, implemented in Random Jungle

(A) Performance of AD-Control classifier in AD and Control samples	Accuracy		Sensitivity		Specificity		PPV (%)	NPV (%)
	Total correctly classified	%	AD correctly classified	%	Control correctly classified	%		
AD-Control training cohort (expression)	128/156	82.1	68/78	87.2	60/78	76.9	79.7	85.7
AD-Control validation cohort (expression)	39/52	75.0	21/26	80.8	18/26	69.2	72.4	78.3
AD-Control validation cohort (expression + imaging)	36/46	78.3	19/23	82.6	17/23	73.9	76.0	81.0
AD-Control validation cohort (imaging)	39/46	84.8	20/23	87.0	19/23	82.6	83.3	86.4
AD-Control validation cohort (expression [in imaging subset])	32/46	69.6	16/23	69.6	16/23	69.6	69.6	69.6
	Mean	95% CI	Mean	95% CI	Mean	95% CI		
AD-Control bootstrapping <sup>a</sup> (expression)	78.2	77.4–79.0	79.6	78.4–80.8	76.8	75.7–77.9		
AD-Control bootstrapping <sup>a</sup> (expression + imaging)	84.0	83.3–84.7	84.4	83.4–85.4	83.5	82.4–84.6		
AD-Control bootstrapping <sup>a</sup> (imaging)	82.0	81.3–82.7	80.0	78.9–81.1	84.0	82.9–85.1		
AD-Control bootstrapping <sup>a</sup> (expression [in imaging subset])	76.0	75.1–76.9	76.4	75.1–77.7	75.4	74.1–76.7		
(B) Performance of AD-Control classifier in MCI samples	Accuracy		Sensitivity		Sensitivity			
	MCI classified as AD-like	%	MCI <sub>c</sub> classified as AD-like	%	MCI <sub>nc</sub> classified as AD-like	%		
MCI cohort (expression)	90/118	76.3	32/41	78.0	58/77	75.3		
MCI cohort (expression + imaging)	57/92	67.8	15/19	78.9	42/73	57.5		
MCI cohort (imaging)	45/92	48.9	12/19	63.2	33/73	45.2		
MCI cohort (expression [in imaging subset])	64/92	69.6	16/19	84.2	48/73	65.8		
	Mean	95% CI	Mean	95% CI	Mean	95% CI		
MCI bootstrapping <sup>a</sup> (expression)	86.0	84.6–87.4	87.2	85.9–88.5	85.5	84.0–87.0		
MCI bootstrapping <sup>a</sup> (expression + imaging)	61.5	61.1–61.9	83.6	79.8–87.4	55.8	55.4–56.2		
MCI bootstrapping <sup>a</sup> (imaging)	47.2	46.8–47.6	71.0	70.0–72.0	41.0	40.6–41.4		
MCI bootstrapping <sup>a</sup> (expression [in imaging subset])	70.4	69.8–71.0	89.0	88.4–89.7	65.6	65.0–66.2		

<sup>a</sup>For bootstrapped data, the mean value and 95% confidence interval (95% CI), measured over 200 models is shown.



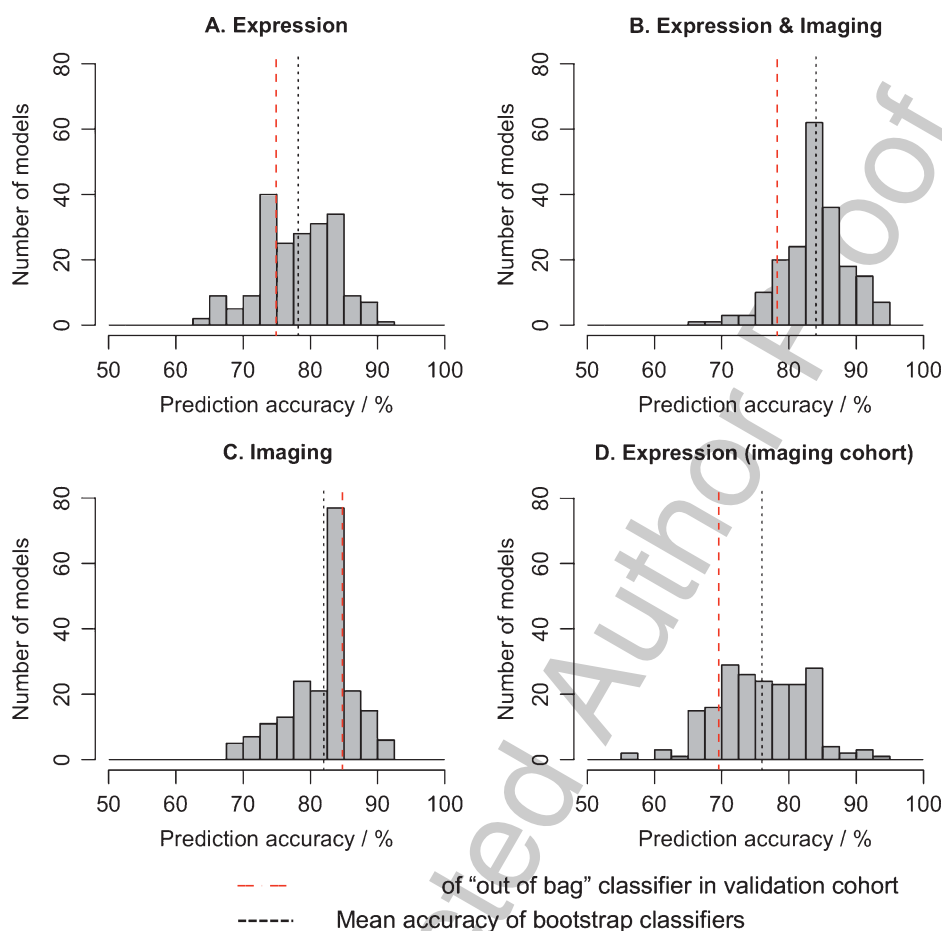


Fig. 2. Bootstrap results for AD-Control classifier in classifying AD and Control samples. The graphs demonstrate the mean accuracy of the classifier measured from bootstrapping (black dotted line) and the accuracy measured using the “out of bag” classifier in the validation cohort (red hashed line). Results are shown for (A) expression classifier alone, (B) expression and imaging classifiers combined, (C) imaging classifier alone, and (D) expression classifier alone in the subset of individuals with sMRI measures.

398 by *t*-tests in the original training cohort. Using this  
 399 method, the accuracy of the expression classifiers  
 400 was slightly higher than we had estimated, with a  
 401 mean accuracy of 78.2% (95% CI, 77.4–79.0%), a  
 402 sensitivity of 79.6% (95% CI, 78.4–80.8%), and a  
 403 specificity of 76.8% (95% CI, 75.7–77.9%) (Fig. 2A;  
 404 Table 3A).

405 Structural MRI is able to accurately detect sub-  
 406 tle changes in the thickness or volume of particular  
 407 brain areas that occur during AD pathogenesis and is  
 408 believed to be associated with the onset of neuronal  
 409 dysfunction and cell loss. We first investigated the  
 410 power of sMRI to classify the AD and control subjects  
 411 using 68 local cortical thickness and 41 brain vol-  
 412 ume MRI measures collected in a subset of our cohort  
 413 around the time of blood sampling [34, 36, 59, 60]  
 414 (Supplementary Table 1). As six patients used in our  
 415 expression validation cohort did not have neuroimag-

416 ing measures, we initially re-evaluated our 203 probes  
 417 on this subset of 46 patients. Accuracy, sensitivity,  
 418 specificity, PPV, and NPV were all 69.6%, indicating a  
 419 small drop in performance in this subgroup. However,  
 420 when bootstrapping, the mean accuracy achieved was  
 421 76.0% accuracy (95% CI, 75.1–76.9%), with a sensi-  
 422 tivity of 76.4% (95% CI, 75.1–77.7%) and specificity  
 423 of 75.4% (95% CI, 74.1–76.7%) (Fig. 2D; Table 3A),  
 424 values similar to that observed in the larger expres-  
 425 sion cohort (Fig. 2A; Table 3A) and demonstrating  
 426 that bootstrapping is important for assessing the true  
 427 variation in accuracy within a population. The sMRI  
 428 measures correctly classified 39 people out of 46 tested  
 429 in the validation cohort (84.8% accuracy), correspond-  
 430 ing to 20 out of 23 AD subjects correctly included  
 431 (87.0% sensitivity), and 19 out of 23 control subjects  
 432 correctly excluded (82.6% specificity) (Table 3A). The  
 433 mean accuracy from bootstrapping was lower (82.0%;

95% CI, 81.3–82.7%), due to fewer AD subjects being correctly classified over the 200 models (80.0% mean sensitivity; 95% CI, 78.9–81.1%), although specificity was slightly improved (84.0% specificity; 95% CI, 82.9–85.1%) (Fig. 2C; Table 3A). The Kappa coefficient was 0.31 ( $p$ -value <0.05) demonstrating good agreement between the imaging and expression classifiers.

Combining the expression and imaging measures resulted in a small increase in mean accuracy following bootstrapping (84.0; 95% CI, 83.3–84.7%) (Fig. 2B; Table 3A). This was due to a small increase in the number of AD subjects being correctly classified (84.4% mean sensitivity; 95% CI, 83.4–85.4%), than achieved with imaging or expression alone.

#### *Performance of diagnostic classifier in MCI subjects*

To evaluate whether our diagnostic blood gene expression classifier could be an early marker of cognitive dysfunction, we tested it in 118 MCI subjects to see how many subjects would be classified as “AD-like” rather than as controls, and whether there was any preference for subjects who subsequently received an AD diagnosis within 2 years ( $MCI_c$ ) compared to those had not received an AD diagnosis ( $MCI_{nc}$ ), but nevertheless were likely to have an AD-endpoint. It categorized the majority of MCI subjects as “AD-like” (90/118 subjects, 76.3%) rather than as controls, which corresponded to 32/41  $MCI_c$  (78.0%) and 58/77  $MCI_{nc}$  (75.3%) (Table 3B). When bootstrapped, the mean accuracy was higher (86.0; 95% CI, 84.6–87.4%), with a similar proportion of  $MCI_{nc}$  and  $MCI_c$  being classified as AD-like (mean 87.2 and 85.5%, respectively) (Fig. 3A; Table 3B).

Although there were only a limited number of  $MCI_c$  subjects with sMRI scans available for analysis (only 19 subjects with imaging compared to 41 available with expression), we assessed the performance of our diagnostic expression classifier in the  $MCI_c$  and  $MCI_{nc}$  groups separately and compared this to the performance with sMRI based models in 92 individuals for which sMRI and expression data were both available. Of the 92 people with MCI, 64 were classified as AD-like (69.6%) using the expression classifier, corresponding to 48/73  $MCI_{nc}$  (65.8%) and 16/19  $MCI_c$  (84.2%). When the sample cohort was bootstrapped, the mean accuracy was 70.4% (95% CI, 69.8–71.0%). Compared to the whole expression cohort, accuracy in this subpopulation was lower and while the mean sensitivity in classifying  $MCI_c$  was high (89.0%; 95% CI,

88.4–89.7%), the mean sensitivity to classify  $MCI_{nc}$  as AD-like was far lower than in the whole population analyzed (65.6%; 95% CI, 65.0–66.2%) (Fig. 3D; Table 3B).

sMRI alone appeared less able to classify  $MCI_c$  as “AD-like” (63.2%) compared to the expression classifier (84.2%), classifying only 12 out of 19 patients as AD-like, suggesting imaging is not as sensitive at identifying potential prodromal AD subjects compared to the expression classifier, even when these individuals were within two years of receiving an AD diagnosis. In the  $MCI_{nc}$  group, the imaging classifier was no better than chance (33/73; 45.2%) at classifying individuals as “AD-like” or control, whereas the expression classifier identified more “AD-like” individuals in the  $MCI_{nc}$  population (65.8%) (Table 3B).

## DISCUSSION

We have shown that there may be potential in using blood expression as a diagnostic classifier for AD. Specifically, we have identified 48 genes (50 probes) which can distinguish between AD and normal elderly control subjects with an accuracy of 75% in a validation cohort. This performance is consistent with previously reported accuracies using blood gene expression measures [31–33] and is similar to other single or multivariate classifiers incorporating measures from CSF and/or neuroimaging [64–68].

No marker would be expected to achieve perfect accuracy when tested in a population of people clinically diagnosed with AD as AD is a very heterogeneous disease with symptoms similar to other dementias and is therefore not always correctly diagnosed by a set of clinical symptoms alone. Clinical diagnosis generally achieves 80–90% accuracy against a postmortem AD diagnosis [54]. Furthermore, some of the pathologically relevant changes detected by a marker may occur before symptoms emerge in apparently normal people, leading to their possible in-life misclassification. Amyloid deposition is not only possible to detect in people with MCI, but is also present in 20–40% of cognitively normal elderly people, up to 10 years before AD diagnosis [11, 14, 15, 20, 69–75]. Some of the normal elderly subjects in our study displayed blood expression changes characteristic of people with AD. Although speculative, this may not be misclassification by the marker, but could instead represent subtle peripheral changes occurring in pre-clinical disease.

Of the 39 genes included in the classifier with known function, eight are associated with mitochondrial

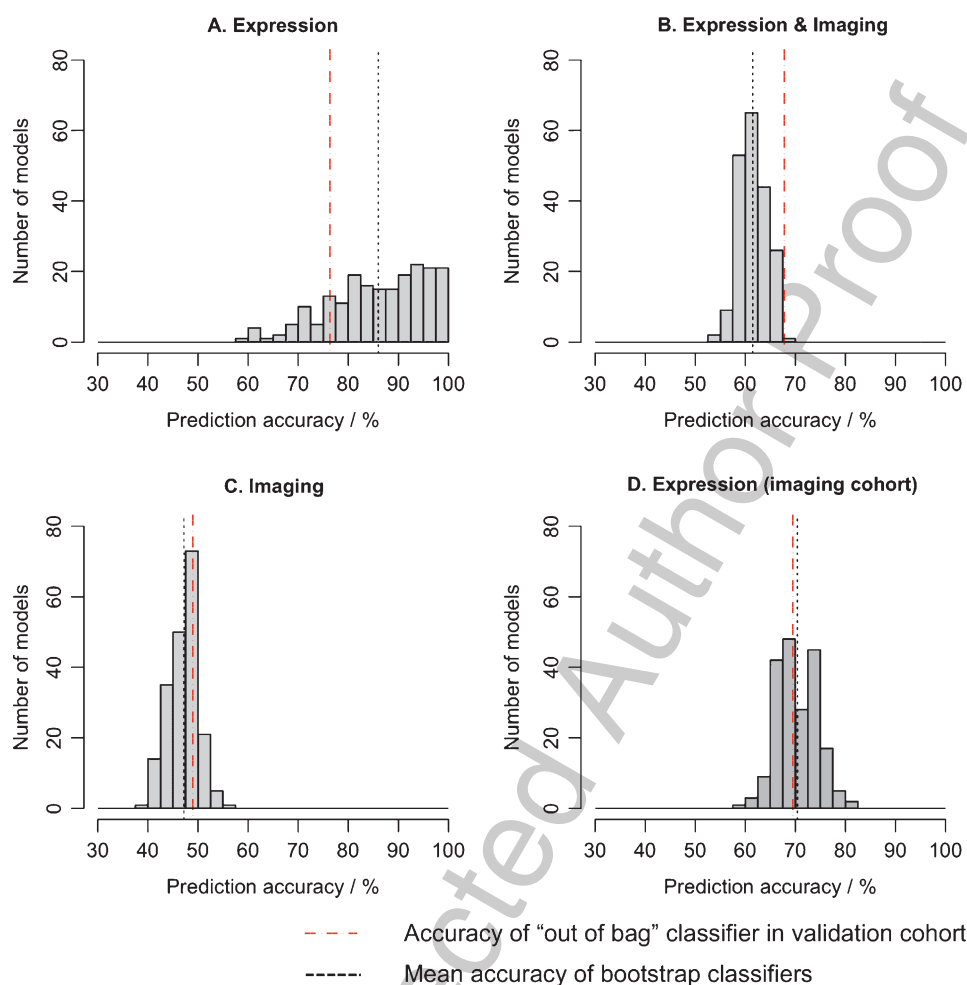


Fig. 3. Bootstrap results for the AD-Control classifier in classifying MCI samples. The graphs demonstrate the mean accuracy of the classifier measured from bootstrapping (black dotted line), and the accuracy measured with the “out of bag” classifier in the validation cohort (red hashed line). Results are shown for (A) expression classifier alone, (B) expression and imaging classifiers combined, (C) imaging classifier alone, and (D) expression classifier alone in the subset of individuals with sMRI measures.

activity and oxidative phosphorylation including subunits of the electron transport chain or constituents of mitochondrial ribosomes and 12 are involved in translation. Changes in the expression of genes associated with these processes in AD blood was recently described in detail by us [76] and genes involved in these processes are enriched in other AD gene expression classifiers [32, 33]. These processes are also significantly altered in the brains of people with AD [77–80], which may represent a common response to the same disease-associated signal(s).

There are a number of limitations to this study, namely the sample size for validation and the lack of additional cohorts to further test the classifier. By performing power calculations using the MVPower R package, we have shown that our sample size has 80%

power with a conservative effect size estimate of 0.2 and 100% with an effect size of 0.7 as derived from our data. We have addressed the second issue by applying a robust bootstrapping approach, considered by the community to be the most appropriate approach for evaluating a classifier when a second cohort is unavailable [61]. When new datasets become available to us we will be able to test the performance of our classifier in additional samples. We are confident that the findings will replicate, as the predictive genes are known to be AD-related and these processes have been previously identified in AD classifier studies, as described above.

In order to further explore the performance of the blood expression classifier we developed, we analyzed measures of cortical thickness and local

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565 brain atrophy determined by MRI where avail- 617  
566 able in the same subjects. Measures of brain 618  
567 atrophy correlate with the severity of cognitive impair- 619  
568 ment and rates of neuronal and synaptic loss in AD [60, 620  
569 81, 82]. Our best neuroimaging classifier achieved an 621  
570 accuracy of 85%, similar to what has been reported 622  
571 previously [34, 83] and only slightly better than the 623  
572 blood expression classifier. Overall these results add 624  
573 weight to the diagnostic validity of using the blood 625  
574 expression classifier we have developed for diagnosing 626  
575 AD independently of information provided by other 627  
576 methods such as structural MRI measures. However, 628  
577 further evaluation is needed to validate its performance 629  
578 in independent samples. 630

579 While a diagnostic marker to back up a clinical diag- 631  
580 nosis of AD is of value, an arguably more important 632  
581 goal is to improve the likelihood of identifying people 633  
582 with prodromal AD as early as possible in the course of 634  
583 their disease, which will reduce variability in clinical 635  
584 trials and allow recruitment and eventually treatments 636  
585 to begin as close as possible to disease onset before 637  
586 irreversible brain changes occur. This is an enormous 638  
587 challenge as there are no obvious transition points to 639  
588 AD. Markers are likely to be far more sensitive at pick- 640  
589 ing up early disease-relevant changes than phenotypic 641  
590 measures. In practice, it is likely that multimodal mark- 642  
591 ers will be used in combination to build up a profile 643  
592 of disease likelihood for each individual. One of the 644  
593 earliest indications of AD pathology that have been 645  
594 reported is decreased CSF  $A\beta_{1-42}$  levels and increased 646  
595 brain  $A\beta$  plaque deposition, which can be observed in 647  
596 pre-clinical disease in some individuals. The connec- 648  
597 tion between CSF  $A\beta_{1-42}$  and AD pathology is well 649  
598 established, with CSF  $A\beta_{1-42}$  correlating with post- 650  
599 mortem plaque [14], tangle number [84], aggregate 651  
600 deposition evaluated by PIB-PET and FDDNP-PET 652  
601 [20], and atrophy measured by CT [85]. 653

602 Pathophysiological changes emerging in the course 654  
603 of AD are believed to be associated with a dynamic 655  
604 temporal sequence of changes in the brain and other 656  
605 biological fluids [12, 86]. Our data adds weight to the 657  
606 body of evidence suggesting there may be potential 658  
607 for markers capturing peripheral blood changes occur- 659  
608 ring in early prodromal AD, as a high percentage of 660  
609 people with MCI who were expected to have a likely 661  
610 AD-endpoint displayed changes sufficiently different 662  
611 from normal to classify them as "AD-like" rather than 663  
612 as controls. The AD classifier appeared to make only a 664  
613 small distinction in favor of classifying MCI subjects 665  
614 who were close to receiving a diagnosis of AD as AD- 666  
615 like than those who did not receive an AD diagnosis 667  
616 over the same short follow-up period of two years. This 668

is in contrast to the performance of the imaging marker 617  
that classified far fewer MCI subjects overall as AD- 618  
like compared to the gene expression classifier, even 619  
those subjects who subsequently received an AD diag- 620  
nosis within two years. This may suggest measures of 621  
structural brain changes have less sensitivity early in 622  
disease compared to the expression marker in blood 623  
we describe, but this will be uncertain until the MCI 624  
non-converters have been followed for a longer period. 625  
Changes detected by sMRI appear to occur at a later 626  
stage of disease than changes in  $A\beta$  and tau [11, 12, 627  
87–89], and it will therefore be important in the future 628  
to evaluate our blood expression classifier alongside 629  
measures of CSF or brain  $A\beta$  to see if the high classi- 630  
fication of AD among the MCI subjects reflects early 631  
detection of prodromal disease and to map the dynamic 632  
onset of changes we observe. 633

634 Due to small sample numbers and therefore insuffi- 635  
cient statistical power when we divided the MCI group 636  
in to those who subsequently received an AD diagno- 637  
sis within two years and those who did not, we were 638  
unable to develop a classifier able to distinguish these 639  
two groups. However, the majority of MCI subjects 640  
had peripheral blood gene expression changes in com- 641  
mon with AD patients including those who did and did 642  
not receive an AD diagnosis within two years. This is 643  
a finding we have previously observed in a study of 644  
cell based proteins in blood comparing AD and MCI 645  
subjects [23] and is similar to the profile of reduced 646  
 $A\beta_{1-42}$  observed in the CSF in some control and many 647  
MCI subjects, which is believed to represent a patho- 648  
physiological process that significantly departs from 649  
normality [37]. Two factors are likely to contribute to 650  
this observation; first, around half of the subjects in 651  
the MCI cohort were selected for analysis because we 652  
knew they had subsequently converted to a probable 653  
AD diagnosis. Second, our MCI sample population are 654  
drawn from specialist memory clinics and are there- 655  
fore more likely to represent people with established 656  
cognitive problems resulting from prodromal AD than 657  
might be expected from a cohort drawn from a com- 658  
munity population, as we previously reported from a 659  
meta-analysis of longitudinal studies of MCI [90]. 660

661 Alternatively, our blood expression marker may rep- 662  
resent an endophenotype shared by a group of diseases 663  
with related etiology. Our two year follow-up period 664  
is insufficient to confirm which of the normal elderly 665  
control or  $MCI_{nc}$  subjects have prodromal AD and 666  
will therefore eventually receive a clinical diagnosis of 667  
AD. Pathological confirmation of an AD diagnosis will 668  
take longer still. We know of no existing studies with 669  
blood collected for RNA purposes where postmortem 670

diagnosis confirming AD would allow such analyses. While confirming the specificity of our marker is an important goal, the existence of an endophenotype, defined here as a disease-associated phenotype not necessarily specific to, or present in all individuals, has clinical relevance. Such a marker can assist in the development of drugs targeting relevant and common disease endophenotypes and does not necessitate unique disease association to achieve efficacy in a relevant disease population. It could also be useful as part of a staged diagnostic approach, providing a cost effective method of identifying individuals with a greater likelihood of developing disease who could subsequently be referred for more expensive diagnostic tests.

Blood is emerging as a very promising tissue in which to achieve a non-invasive and relatively inexpensive assay for detection of AD. In addition to changes in blood gene expression [31–33, 91], plasma protein panels have been described which accurately distinguish AD from normal elderly control people and/or MCI subjects who convert from those who remain stable, or to predict disease progression [92]. There are also many reports of individual proteins with altered abundance in plasma in AD and normal elderly control groups, suggesting blood is a realistic tissue in which to identify markers of AD [23, 93–102]. However, there are still technical issues to overcome as not all protein measures reliably change across studies [103]. In the future, it will be important to explore the performance of different combinations of measures to achieve the most accurate biomarker for diagnosis and make comparisons between blood markers and more established biomarkers linked to pathophysiology and establish their relative temporal patterns of change during disease progression in relation to these other biomarkers.

In conclusion, we have shown that peripheral blood shows promise as an AD-associated diagnostic blood gene expression marker that may be useful very early in pre-clinical disease. It performed similarly to using neuroimaging measures alone in AD and normal elderly control samples. Future work will evaluate this blood expression marker in subjects from which CSF measures of A $\beta$ <sub>1-42</sub> and/or PET amyloid have been measured in order to further explore the specificity and timing of these changes. The existence of such a marker in an accessible tissue such as blood would contribute significantly toward efforts to identify and treat people with AD very early in their disease before significant neuronal loss has occurred. For example, CSF A $\beta$ <sub>1-42</sub> and tau measurements to enrich for likely

AD are predicted to reduce sample size by 67% and costs by 60% in a clinical trial compared to a trial with unselected MCI subjects [104]. Evaluation of the marker in related diseases will establish whether the changes we see are specific to AD or are shared across similar diseases. A lack of disease specificity would not diminish the value of a marker able to capture a common disease-associated endophenotype for which a specific treatment with real clinical value could be developed.

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Authors' disclosures available online (<http://www.j-alz.com/disclosures/view.php?id=1502>).

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